

ORIGINAL ARTICLE

Open Access



# Using the Bair Hugger™ temperature monitoring system in neck and chest regions: a pilot study

Shunsuke Tachibana\* , Yutaro Chida and Michiaki Yamakage

## Abstract

**Purpose:** Temperature monitoring in the perioperative periods is important in order to avoid both hyperthermia and hypothermia. In our pilot study, we evaluated the usefulness of Bair Hugger™ temperature monitoring system (BHTMS), a forehead deep temperature monitoring system, in the neck and chest under general anesthesia.

**Methods:** After approval from the Sapporo Medical University Research Ethics Board, 30 female patients scheduled for laparoscopic surgery were enrolled in this study. Patients were divided into three groups, depending on the attachment regions of BHTMS sensor. Temperatures obtained from the three regions and each esophageal temperature ( $T_{\text{Eso}}$ ) were monitored and analyzed.

**Results:** A Bland-Altman plot showed that the mean bias between temperature obtained from the neck and  $T_{\text{Eso}}$  was +0.05 °C above  $T_{\text{Eso}}$  ( $2\text{SD} \pm 0.35$  °C), and that between temperature obtained from the chest and  $T_{\text{Eso}}$  was -0.55 °C above  $T_{\text{Eso}}$  ( $2\text{SD} \pm 0.55$  °C).

**Conclusion:** By using the BHTMS sensor in the neck region, it is possible to monitor core body temperature seamlessly and with high reliability. These results may suggest that the use of BHTMS has high versatility in measuring perioperative core body temperature.

**Trial registration:** This study was approved by the Sapporo Medical University Research Ethics Board (2015: No. 262-149) and registered with UMIN Clinical Trial Registry ([UMIN000016802](https://clinicaltrials.gov/ct2/show/study/UMIN000016802) Registered 15 March 2015).

**Keywords:** Perioperative body temperature monitoring, Bair Hugger™ temperature monitoring system, Non-cardiac surgery

## Background

Temperature monitoring in the perioperative periods is important in order to avoid both hyperthermia and hypothermia. Malignant hyperthermia, the phenomenon of hyperthermia during use of volatile anesthetics and succinylcholine, requires monitoring and urgent treatment for the drastic temperature elevation [1, 2]. Perioperative hypothermia is also known to be harmful to patients because it can cause adverse events such as life-threatening arrhythmia [3], higher risk of surgical site infection (SSI) [4], abnormal hemostasis [5, 6], a

possibility of massive hemorrhage [7], and harmful shivering [8, 9].

During surgery, core body temperature is usually monitored in the rectum, bladder, and ear. However, temperatures obtained from these body regions sometimes poorly reflect the real values and drastic changes in core body temperature [10–12]. As another way of monitoring core temperature, we may select zero-heat-flux thermometer which can measure deep temperature approximately 1–2 cm below the skin surface [13]. In Japan, we can use the Bair Hugger™ temperature monitoring system (BHTMS; 3M, St. Paul, MN, USA), which involves attachment of a thermal sensor on the forehead throughout the perioperative period. It was proved that this monitoring device is highly reliable for core body temperature monitoring [14, 15]. However, application

\* Correspondence: [shunsuke.tachibana@gmail.com](mailto:shunsuke.tachibana@gmail.com)

Department of Anesthesiology, Sapporo Medical University, School of Medicine, Sapporo, South 1, West 16, Chuo-ku, Sapporo, Hokkaido 060-8543, Japan

of the BHTMS remains problematic in certain clinical situations. For example, in craniotomy and neck or face surgeries, we cannot attach the forehead sensor on patients' frontal head region. The forehead sensor is also difficult to apply when the frontal head region is covered by the other probes such as depth of anesthesia or tissue oxygen saturation monitors.

Hence, we attached the forehead sensor to other body regions and continuously compared with the esophageal temperature which is highly reliable for core body temperature [16, 17]. The aim of this study is to evaluate the performance of BHTMS in the neck and chest in Japanese patients who were scheduled non-cardiac surgery.

### Materials and methods

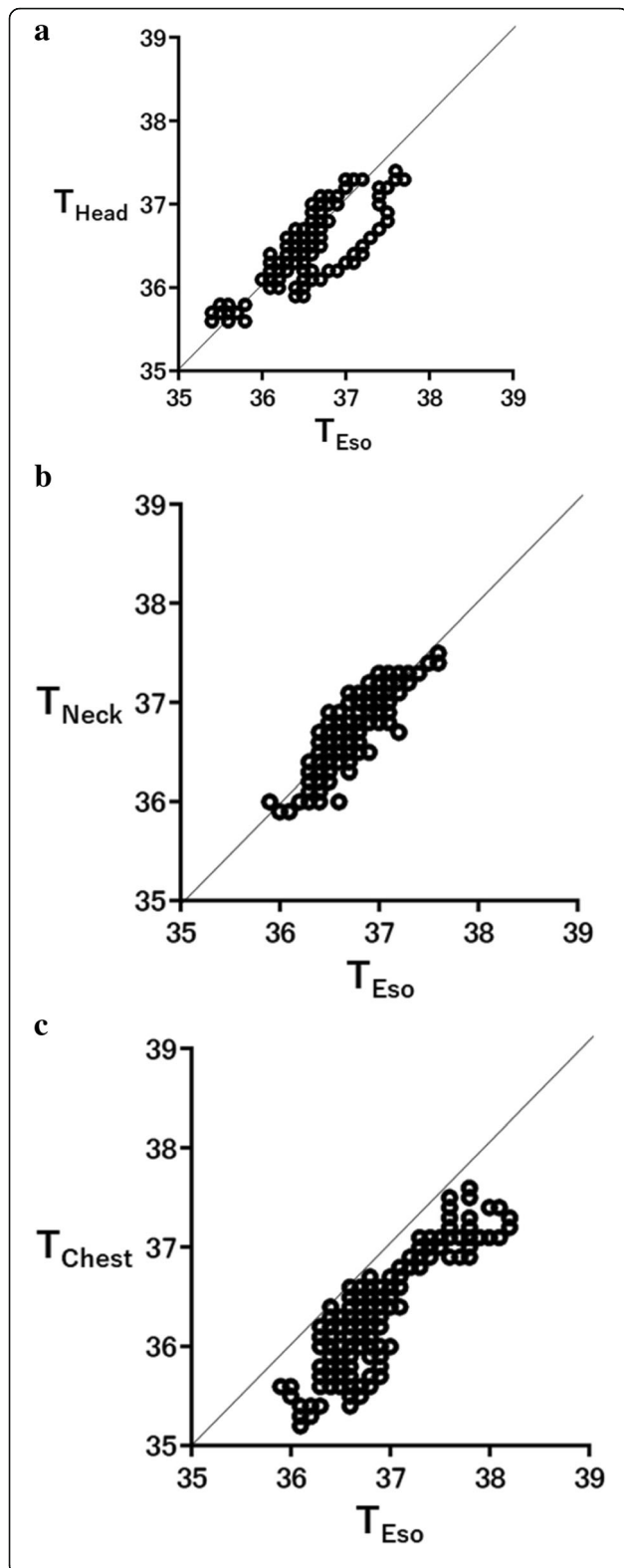
This study was approved by the Sapporo Medical University Research Ethics Board (2015, No. 262-149; Chairperson, N. Masumori), and written informed consent was obtained from each participant. The trial was registered at the UMIN Clinical Trials Registry (UMIN000016802) before patient recruitment. Eligible participants were 30 female patients between 21 and 80 years old who had scheduled laparoscopic surgery under general anesthesia except for upper gastrointestinal tract surgeries. The patients enrolled in this study (American Society of Anesthesiologist physical status 1–3) have no esophageal lesions and/or no abnormalities in the region of attachment and were not expected to be suffering from massive hemorrhage during surgery. We divided the participants into three groups—the forehead group ( $N = 10$ ), neck group ( $N = 10$ ), and anterior chest group ( $N = 10$ ) due to different attachment regions of BHTMS sensor. None of the patients received premedication before entering the operation room. In the operation room, a 20G intravenous catheter was inserted into the light forearm and bicarbonate Ringer's solution fluids warming at 37.0 °C started to infuse. General

anesthesia was induced by using propofol (1.5–2.0 mg/kg) and fentanyl (1.0–2.0 µg/kg) and the tracheal intubation was performed after injecting 0.9 mg/kg rocuronium. After intubation, esophageal temperature probe (Novatemp®; NOVAMED, NY, USA) was properly inserted into the esophagus under observing by McGrath®MAC (Aircraft Medical CO., LTD, UK). We located the temperature probe tip in the lower esophagus and the distance was predicted in advance by referring to patients' chest radiograph. And then, BHTMS sensor was placed on the light forehead in forehead group, above the left common carotid artery in the neck group, and on the 4 left sternal borders in the anterior chest group. After setting the thermometers, we performed the ultrasound-guided transversus abdominis plane block or quadratus lumborum block using 0.375% ropivacaine (dose within 3.0 mg/kg) as postoperative pain control. These processes of general anesthesia induction were performed by either two experienced anesthesiologists. Anesthesia during the operation was maintained with 1.5% sevoflurane in 3 L/min air and 1 L/min oxygen with 0.1–0.2 µg/kg/min remifentanyl continuous administration. The ambient temperature was maintained approximately at 23.0 °C and the humidity at 40% during operation. Approximately 60 min before the end of the surgery, 1000 mg acetaminophen was intravenously administered. Esophageal temperature ( $T_{Eso}$ ) and temperature obtained from three locations ( $T_{Head}$ ,  $T_{Neck}$ ,  $T_{Chest}$ ) were monitored and continuously recorded to a laptop computer at 5-min intervals until just before discontinuation of sevoflurane exposure. Anesthesiologist in attendance appropriately used a forced-air warming system (Bair Hugger™ patient warming Model 750; 3M, MN, USA) and blankets (patient warming Model 522 and Model 545; 3M, MN, USA), warmed the patients at 43 °C during general anesthesia.

One-way ANOVA was used to compare the patients' background differences of age, height, weight, and body mass index (BMI). Kruskal-Wallis test was used to

**Table 1** The admission characteristics of participants in each group. Data are represented as mean ± SD, medians (interquartile ranges [IQR]), or absolute number. There was no significant difference in each group statistically

Admission characteristics	Forehead group (n=10)	Neck group (n=10)	Anterior chest group (n=10)
Age (year)	49.3 ± 15.9	43.4 ± 14.7	58.6 ± 17.9
Height (cm)	162.7 ± 12.3	163.4 ± 10.2	157.2 ± 7.9
Weight (kg)	61.1 ± 9.9	67.3 ± 23.9	58.2 ± 10.0
BMI (kg/m <sup>2</sup> )	22.9 ± 2.1	24.7 ± 5.8	23.5 ± 3.7
Sex (M/F)	4/6	5/5	4/6
ASA-PS ( I / II / III)	4/6/0	3/6/1	2/7/1
Duration of surgery (min)	147 [105-181]	204 [126-344]	195 [98-266]
Duration of anesthesia (min)	213 [174-233]	255 [172-413]	253 [214-387]
Blood loss (ml)	25 [0-70]	75 [50-156]	0 [0-5]
Estimated water balance (ml)	740 [662-1257]	1020 [650-1978]	975 [630-2335]



**Fig. 1** Pearson's correlation between esophageal temperature and other temperatures. **a** Plots of temperature data obtained from the forehead ( $T_{Head}$ ) and esophagus ( $T_{Eso}$ ), **b** neck ( $T_{Neck}$ ) and  $T_{Eso}$ , and **c** anterior chest ( $T_{Chest}$ ) and  $T_{Eso}$ . Thin lines in the figure denote the line of identity. Pearson's correlation coefficient indicated a strong correlation for all comparisons ( $r=0.81$  between  $T_{Eso}$  and  $T_{Head}$ ,  $r=0.86$  between  $T_{Eso}$  and  $T_{Neck}$ , and  $r=0.84$  between  $T_{Eso}$  and  $T_{Chest}$ )

compare the differences of the length of operation time, length of anesthesia time, blood loss, and estimated water balance.  $P$  values  $< 0.05$  were considered to indicate significant differences. Each of  $T_{Head}$ ,  $T_{Neck}$ , and  $T_{Chest}$  were evaluated in comparison with  $T_{Eso}$  as a core body temperature. Pearson's correlation and Bland-Altman plots were used to compare  $T_{Eso}$  and  $T_{Head}$ ,  $T_{Eso}$  and  $T_{Neck}$ , and  $T_{Eso}$  and  $T_{Chest}$ . Bland-Altman plots were used to evaluate the limits of agreement (LOA) between  $T_{Eso}$  and  $T_{Head}$ ,  $T_{Eso}$  and  $T_{Neck}$ , and  $T_{Eso}$  and  $T_{Chest}$ . Considered to several past articles about body temperature monitoring, the mean value of the difference (bias)  $< 0.4^{\circ}\text{C}$  and 2 standard deviations (SD)  $< \pm 1.0^{\circ}\text{C}$  was defined statistically significant in this study. All statistical analyses were performed using Prism software version 6 for Windows (GraphPad Software Inc., La Jolla, CA, USA).

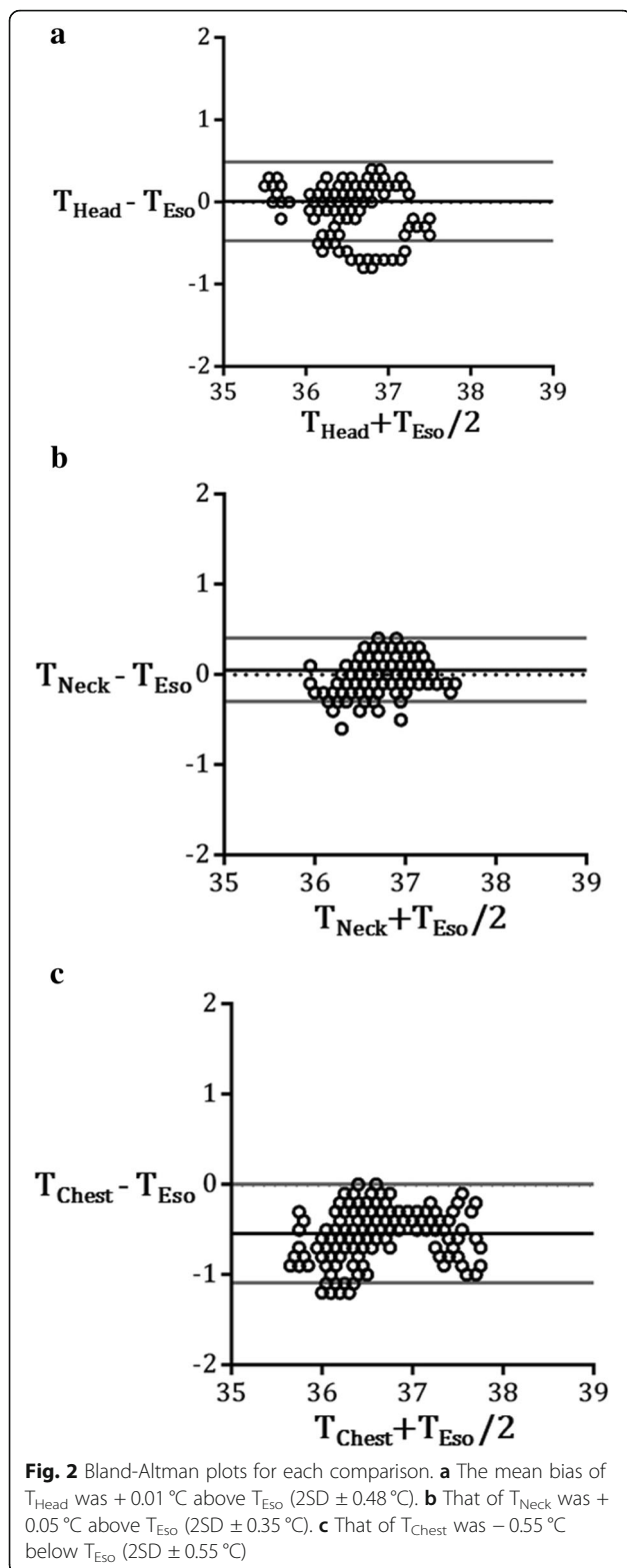
## Results

We totally obtained 303, 446, and 487 data pairs for the comparisons of  $T_{Eso}$  and  $T_{Head}$ ,  $T_{Eso}$  and  $T_{Neck}$ , and  $T_{Eso}$  and  $T_{Chest}$ , respectively. No monitoring defect caused by electronic devices was observed in this study. There were no significant differences in age, height, weight, BMI, length of operation, length of anesthesia, blood loss, and estimated water balance in each group (Table 1). Figure 1 a–c show Pearson's correlation coefficient ( $r$ ) in each comparison. Pearson's correlation coefficients were 0.81, 0.86, and 0.84 between  $T_{Eso}$  and  $T_{Head}$ ,  $T_{Eso}$  and  $T_{Neck}$ , and  $T_{Eso}$  and  $T_{Chest}$ , respectively, indicating a strong correlation in all comparisons (Fig. 1).

Figure 2a–c show the Bland-Altman plot between  $T_{Eso}$  and the other temperature values. The mean bias of BHTMS with normal forehead usage was  $+0.01^{\circ}\text{C}$  above the  $T_{Eso}$  with  $\pm 0.48^{\circ}\text{C}$  2SD. The mean biases of  $T_{Neck}$  and  $T_{Chest}$  were  $+0.05^{\circ}\text{C}$  above  $T_{Eso}$  with 2SD of  $\pm 0.35^{\circ}\text{C}$ , and  $-0.55^{\circ}\text{C}$  below  $T_{Eso}$  with 2SD of  $\pm 0.55^{\circ}\text{C}$ , respectively (Fig. 2). There were no complications related to the location of esophageal probe insertion and of BHTMS sensor attachment in any of the cases.

## Discussion

Perioperative temperature monitoring is an essential factor as with other vital signs—blood pressure, heart rate, and percutaneous oxygen saturation. For accurate temperature measurements, we must select the kind of



thermometers, insertion, or attachment regions [18, 19]. Perioperative hypothermia causes a higher risk of SSI [4], massive hemorrhage [7], and postoperative shivering [8, 9]. For prevention of evitable hypothermia during

surgery, we must accurately monitor core body temperature and effectively perform body warming.

Usefulness of zero-heat-flux thermometer has been already reported in perioperative temperature monitoring. Fox and Solman first reported a principle of an electronic servo-controlled system to achieve almost complete thermal insulation [20]. Zero-heat-flux thermometer sensor contains two thermistors, separated by a thermal insulator and covered by an electric heater. BHTMS, one of the zero-heat-flux thermometers, also has some advantages to use in its accuracy, ease of use, and disposable sensor compared with former types. Eshraghi showed that the overall difference between the temperature obtained from BHTMS and that of the pulmonary artery was  $-0.23\text{ }^{\circ}\text{C}$  (95% LOA of  $\pm 0.82\text{ }^{\circ}\text{C}$ ) [14]. However, this thermometer is unsuitable for use in certain clinical situations. In patients undergoing craniotomy, it is impossible to attach the BHTMS sensor to the patients' forehead. During surgery of the neck and face, as well, surgeons do not permit the BHTMS sensor to be attached due to the proximity of the forehead to the surgical site. Use of a BIS monitor sensor and/or INVOS™ sensor on the patients' forehead is common during cardiovascular surgery, which interferes with the attachment of the BHTMS sensor on the forehead. Since temperature monitoring is more significant in the surgeries described above, an alternative method to use the BHTMS for the measurement of core body temperature is required. Judging from the principle of the zero-heat-flux thermometer, we hypothesized that core body temperature would be measurable by attaching the BHTMS sensor to other areas with good vascularity. In this pilot study, we could prove a high correlation and accurate performance in the neck group. Eshraghi also presented that bias and precision values for neck site were similar to the forehead values [14]. It was almost comparable performance between standard forehead attachment and neck attachment. Furthermore, the systematic error was absent in the neck group. There are several reasons why core temperature monitoring in the neck is appropriate. The neck is anatomically close to the heart and is a route to the cerebral blood flow; therefore, the blood temperature hardly decreases. Besides, blood vessels in the neck run 1–2 cm below the skin, which has little influence by fatty tissues, making it easier to measure core temperature accurately.

Meanwhile, the mean bias was  $-0.55\text{ }^{\circ}\text{C}$  in the chest group, which had a systematic error. LOA in this systematic error ranged from  $-1.04\text{ }^{\circ}\text{C}$  (lower coefficient limit) to  $-0.06\text{ }^{\circ}\text{C}$  (upper coefficient limit), it is necessary to consider how to interpret numerical values under real clinical use. One reason for systematic error with anterior chest application might be influenced by the effect of the rib bones and pericardial fatty tissue, and

movements of the thoracic cage and aerated lung during breathing.

Our study has certain limitations. First, we monitored and analyzed core body temperature within a limited range, almost between 35.5 and 38.0 °C, in laparoscopic surgery cases. Thus, we cannot judge whether our monitoring method is proper in hyperthermia cases over 38.0 °C and hypothermia cases below 35.5 °C. Second, we collected 10 cases and data from each group, but the sample size was too small. Third, we did not measure peripheral temperature in this study, to serve as a comparison. We need further verifications to resolve these limitations; however, the knowledge obtained from this study would be one option in monitoring core body temperature.

## Conclusions

To conclude, it is possible to monitor core body temperature seamlessly and with high reliability by using the BHTMS in the neck region. Usefulness of BHTMS in the neck is equivalent to that in the original frontal head region. The value measured in the chest has a systematic error, and it is necessary to judge by considering the LOA. In addition, these results from this pilot study suggest that using BHTMS may be more versatile in measuring perioperative core body temperature.

## Abbreviations

BHTMS: Bair Hugger™ temperature monitoring system; BMI: Body mass index; LOA: Limits of agreement;  $T_{\text{Chest}}$ : Temperature obtained from the anterior chest;  $T_{\text{Esoph}}$ : Esophageal temperature;  $T_{\text{Head}}$ : Temperature obtained from the forehead;  $T_{\text{Neck}}$ : Temperature obtained from the neck

## Acknowledgements

Not applicable

## Funding

No funding

## Availability of data and materials

They are available as an Excel® file on reasonable request.

## Authors' contributions

ST designed the experiments; collected, analyzed, and reviewed the data; and wrote the first draft of the manuscript. YC collected data and jointly developed the structure and arguments for the paper. MY made critical revisions and contributed to the writing of the manuscript. All authors approved the final manuscript.

## Ethics approval and consent to participate

This study was approved by the Sapporo Medical University Research Ethics Board (2015: No. 262-149) and registered with UMIN Clinical Trial Registry (UMIN trial ID: UMIN000016802, registered March 15, 2015).

## Consent for publication

Not applicable

## Competing interests

The authors declare that they have no competing interests.

## Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Received: 31 March 2019 Accepted: 29 April 2019

Published online: 16 May 2019

## References

- Hopkins PM. Malignant hyperthermia: pharmacology of trigger. *Br J Anaesth.* 2000;107:48–56.
- Wappler F, Fiege M, Schulte am Esch J. Pathophysiological role of the serotonin system in malignant hyperthermia. *Br J Anaesth.* 2001;87:794–8.
- Frank SM, Fleisher LA, Breslow MJ, Higgins MS, Olson KF, Kelly S, Beattie C. Perioperative maintenance of normothermia reduces the incidence of morbid cardiac events. A randomized clinical trial. *JAMA.* 1997;277:1127–34.
- Kurz A, Sessler DI, Lenhardt R. Perioperative normothermia to reduce the incidence of surgical-wound infection and shorten hospitalization. Study of Wound Infection and Temperature Group. *N Engl J Med.* 1996;334:1209–15.
- Rohrer MJ, Natale AM. Effect of hypothermia on the coagulation cascade. *Crit Care Med.* 1992;20:1402–5.
- Michelson AD, MacGregor H, Barnard MR, Kestin AS, Rohrer MJ, Valeri CR. Reversible inhibition of human platelet activation by hypothermia in vivo and in vitro. *Thromb Haemost.* 1994;71:633–40.
- Schmied H, Kurz A, Sessler DI, Kozek S, Reiter A. Mild hypothermia increases blood loss and transfusion requirements during total hip arthroplasty. *Lancet.* 1996;347:289–92.
- Sessler DI, Israel D, Pozos RS, Pozos M, Rubinstein EH. Spontaneous post-anesthetic tremor does not resemble thermoregulatory shivering. *Anesthesiology.* 1988;68:843–50.
- Frank SM, Fleisher LA, Olson KF, Gorman RB, Higgins MS, Breslow MJ, Sitzmann JV, Beattie C. Multivariate determinants of early postoperative oxygen consumption in elderly patients. Effects of shivering, body temperature, and gender. *Anesthesiology.* 1995;83:241–9.
- Severinghaus JW. Temperature gradients during hypothermia. *Ann N Y Acad Sci.* 1959;80:515–21.
- Benzinger M. Tympanic thermometry in surgery and anesthesia. *JAMA.* 1969;209:1207–11.
- Frank SM, Nguyen JM, Garcia CM, Barnes RA. Temperature monitoring practices during regional anesthesia. *Anesth Analg.* 1999;88:373–7.
- Yamakage M, Namiki A. Deep temperature monitoring using a zero-heat-flow method. *J Anesth.* 2003;17:108–15.
- Eshraghi Y, Nasr V, Parra-Sanchez I, Van Duren A, Botham M, Santoscoy T, Sessler DI. An evaluation of a zero-heat-flux cutaneous thermometer in cardiac surgical patients. *Anesth Analg.* 2014;119:543–9.
- Mäkinen MT, Pesonen A, Jousela I, Päiväranta J, Poikajärvi S, Albäck A, Salminen US, Pesonen E. Novel zero-heat-flux deep body temperature measurement in lower extremity vascular and cardiac surgery. *J Cardiothorac Vasc Anesth.* 2016;30:973–8.
- Moran DS, Mendal L. Core temperature measurement: methods and current insights. *Sports Med.* 2002;32:879–85.
- Sessler DI. A proposal for new temperature monitoring and thermal management guidelines. *Anesthesiology.* 1998;89:1298–300.
- Yamakage M, Kawana S, Watanabe H, Namiki A. The utility of tracheal temperature monitoring. *Anesth Analg.* 1993;76:795–9.
- Cattaneo CG, Frank SM, Hesel TW, El-Rahmany HK, Kim LJ, Tran KM. The accuracy and precision of body temperature monitoring methods during regional and general anesthesia. *Anesth Analg.* 2000;90:938–45.
- Fox RH, Solman AJ, Isaacs R, Fry AJ, MacDonald IC. A new method for monitoring deep body temperature from the skin surface. *Clin Sci.* 1973;44: 81–6.